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(12) United States Patent Elaz et al.

(54) SYSTEM FOR MANAGING VENTILATOR OPERATION

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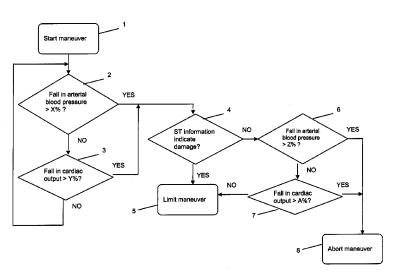
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(57) ABSTRACT

A method for managing patient ventilator operation includes receiving data representing one or more hemodynamic parameters. In response to the received data representing the one or more hemodynamic parameters, one or more commands are provided for adaptively altering ventilator operation.

20 Claims, 6 Drawing Sheets



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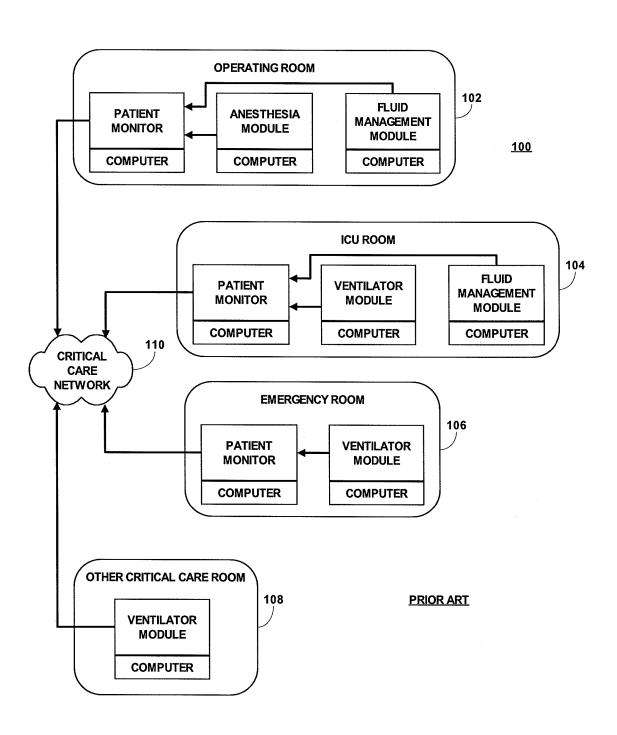


Fig. 1

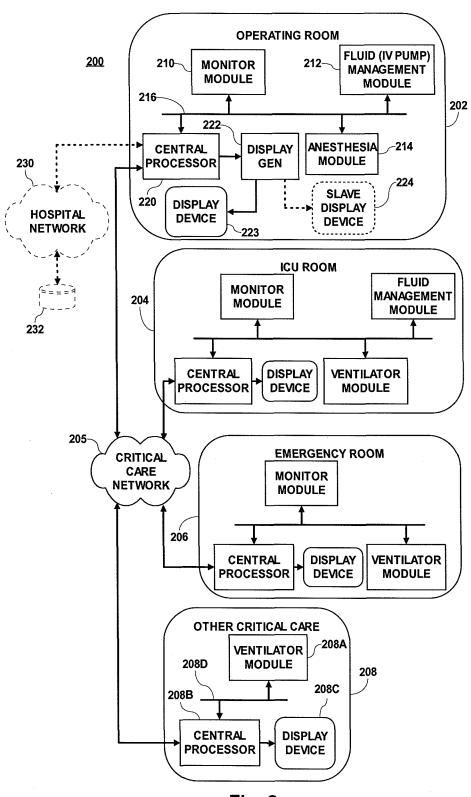


Fig. 2

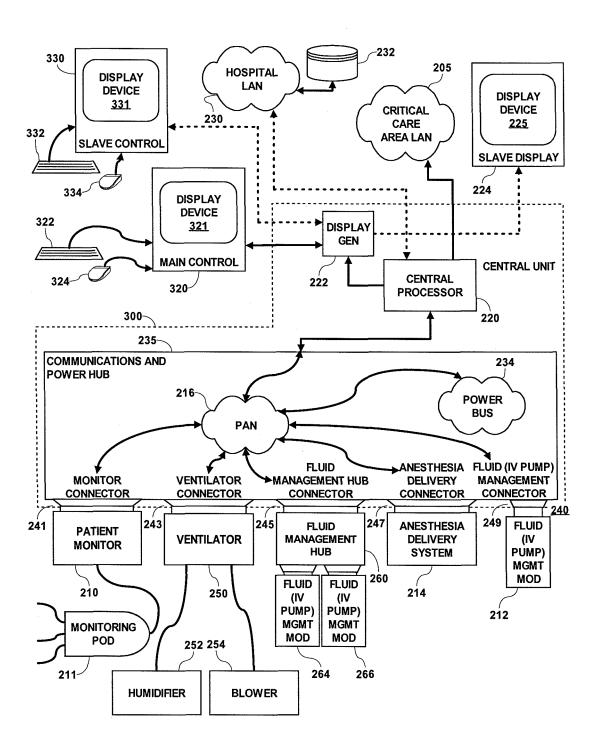


Fig. 3

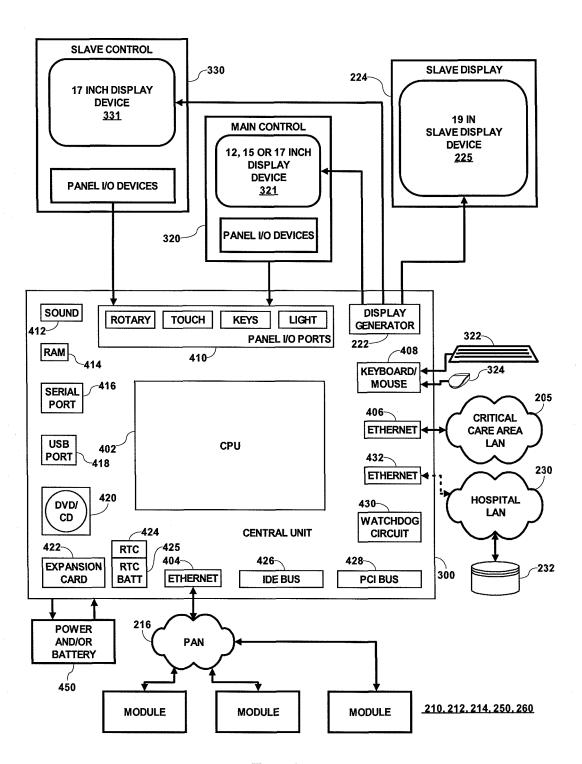


Fig. 4

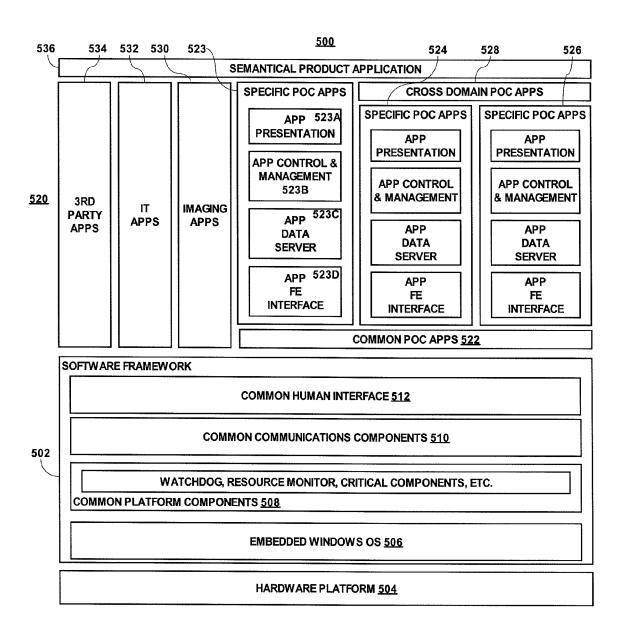
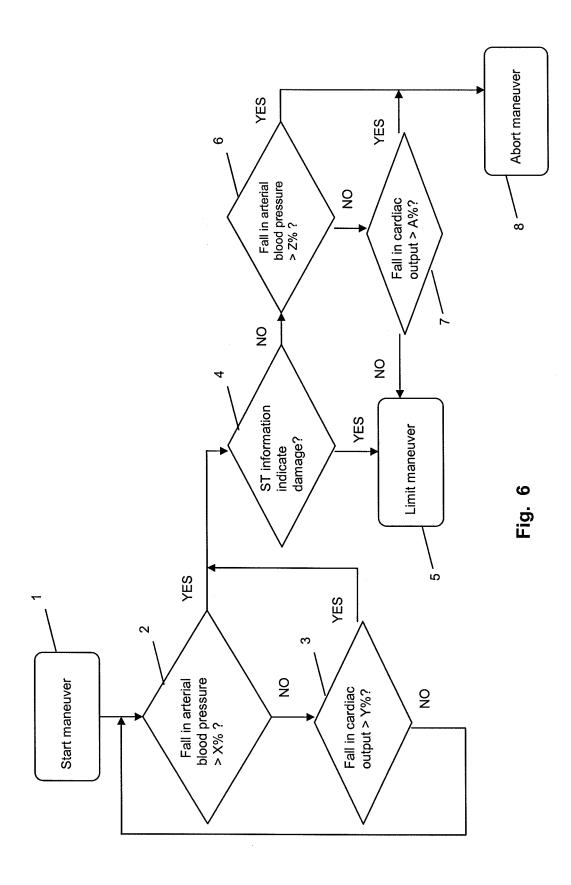


Fig. 5



SYSTEM FOR MANAGING VENTILATOR **OPERATION**

CROSS REFERENCE TO RELATED APPLICATIONS

The application is a continuation-in-part of U.S. patent application Ser. No. 10/976,025 filed Oct. 28, 2004 now abandoned which, in turn, claims priority to U.S. Patent Application No. 60/519,300 filed on Nov. 12, 2003.

FIELD OF THE INVENTION

The present invention relates to a processing device and display system, and in particular to a method and a system for 15 incorporating hemodynamic and electrophysiological information into ventilation maneuvers.

BACKGROUND OF THE INVENTION

Hospitals routinely monitor physiological parameters of patients from first entry until final release. Originally, this was performed by one or more patient monitoring devices, such as a heart rate monitor, an EKG monitor, an SpO2 monitor, and so forth. These physiological parameters were separately 25 detected by separate pieces of equipment, possibly manufactured by respectively different manufacturers. The monitoring equipment included the connections to the patient necessary to measure the physiological parameter and a display device of the type necessary to display the physiological 30 parameter in an appropriate manner. A healthcare worker, such as a nurse, visited the patient's location and looked at each separate system to accumulate the patient's vital signs.

Current systems have integrated measurement of some of the physiological parameters (e.g. EKG, SpO₂, etc.) into a 35 single patient monitoring device. Such a device includes the patient connections necessary to measure the physiological parameters measurable by the device and a display device which can display the measured physiological parameters in an appropriate manner. Such patient monitors may be con- 40 sidered to be partitioned into two sections. A first, operational, section controls the reception of signals from the electrodes connected to the patient and performs the signal processing necessary to calculate the desired physiological parameters. A second, control, status and communication, 45 section interacts with a user to receive control information and with the operational section to receive the physiological parameters, and displays status information and the values of the physiological parameters in an appropriate manner. Either or both of these sections may include a computer or processor 50 to control the operation of that section. This approach has an economic advantage since the control, status and communication section is shared among the parameter monitoring functions.

hospital computer system via a hospital network. In this manner, data representing patient physiological parameters may be transferred to the central hospital computer system for temporary or permanent storage in a storage device. Data received from the patient monitors may also be monitored by 60 a person, such as a nurse, at the central location. The stored data may be retrieved and analyzed by other healthcare workers via the hospital network. Patient monitors in such a networked system include a terminal which is capable of being connected to and communicating with the hospital network. 65 In such a patient monitor, the control, status and communication section controls the display of the physiological

2

parameters, and also the connection to the hospital network and the exchange of the physiological parameters with other systems, such as other patient monitors and/or the central computer storage device, via the hospital network.

Such patient monitoring modules may also be portable. That is, they may operate while being transported with a patient who is being moved from one location to another in the hospital, for example, between a patient room and a therapy or operating room. A portable patient monitor consists of a base unit, and a portable unit which may be docked and undocked from the base unit. Base units may be placed at appropriate locations in the hospital. They are permanently connected to the hospital network and receive power from the power mains. The portable unit includes the necessary patient connections, connections for docking with base units, and a display screen. The portable unit also includes a processor which controls the operation of the portable unit The portable unit further includes a battery and an internal memory device.

While the portable unit of the patient monitor is docked, the 20 batteries are recharged, and data representing physiological parameters are transmitted to the central hospital computer through the base unit via the hospital network. While the portable unit of the patient monitor is undocked, it runs on battery power. During transportation, the patient monitor continues to receive and display physiological parameters, and stores a record of those parameters in the internal memory device. If a base unit is available at the destination, the portable unit may be docked there. Communications is reestablished with the hospital central computer, and battery recharging commenced. At this time, data representing the previously stored parameters is retrieved from the internal memory device and transmitted to the storage device in the central hospital computer via the hospital network.

In such a patient monitor, the control, status and communication section controls display of the physiological parameters and communication of those parameters to the hospital network via the docking unit, and also detection of docking and undocking, control of power (either from the base unit when docked or the internal battery when undocked), storage of physiological parameter data in internal memory when the patient monitor is undocked, and transmission of stored physiological parameter data when the patient monitor is redocked.

Patient monitors have also been adapted to be used to transmit information to the hospital network from other modules. These modules may be patient monitoring modules measuring physiological parameters which are not measured by the patient monitor, or patient treatment modules reporting the status of treatments being provided to the patient. Such patient monitors include input terminals, or wireless input ports, to which these other monitoring modules are connected. Information from these modules is passed through the patient monitor to the hospital network through the base unit.

FIG. 1 is a block diagram of a hospital 100 operating in the Such patient monitors may also be connected to a central 55 manner described above. In FIG. 1, four rooms in a hospital are illustrated: an operating room 102, an intensive care unit (ICU) room 104, an emergency room 106 and another critical care room 108. The operating room 102, the ICU room 104 and the emergency room 106 include a patient monitor device as described above. Each patient monitor includes a connection to a critical care area network 110, either directly from the patient monitor or through a base unit (not shown). Each patient monitor also includes patient connections to electrodes attachable to the patient, not shown to simplify the figure. The patient monitors also receive data from other devices and forward that data to the critical care area network. In the operating room 102, an anesthesia device and fluid

management device are coupled to the critical care area network 110 through the patient monitor; in the ICU room a ventilator device and fluid management device are coupled to the critical care area network 110 through the patient monitor; and in the emergency room 106 a ventilator device is coupled 5 to the critical care area network 110 through the patient monitor. In the other critical care room 108 a ventilator device is coupled directly to the critical care area network 110, either directly or through its own base unit.

The modules illustrated in FIG. 1 operate independently of 10 each other, and each includes its own computer or processor controlling the module. This requires the presence of a base unit for each separate module. In an operating room, where many such modules may be in use concurrently, this requires space, and power. Further, each device may be docked in a 15 base unit for that type of device. That is, a patient monitor device may be docked in a patient monitor base unit, a fluid monitoring device may be docked in a fluid monitoring device base unit, and so forth.

A patient monitor is passive in the sense that it monitors 20 physiological parameters of the patient to which it is attached. However, other medical devices are active in the sense that their operation affects the patient in some manner. For example, the anesthesia device controls the administration of anesthesia to a patient, e.g. during an operation; the fluid 25 management device controls the administration of fluids (blood, saline, and/or medication) to a patient; the ventilator device assists or controls breathing of a patient, e.g. during an operation, and so forth. The active devices also include a computer or processor which controls the operation of the 30 device. These devices also may be connected to a hospital network through a base unit. This allows a central location to monitor and to control the active device. As with the patient monitoring device, an active device, such as a fluid monitoring device, may be portable in the sense that a control module, 35 including a processor, may be undocked from a fixed unit. This control module continues to operate the device, at the last received control settings, e.g. while a patient is transported from one location to another. When at the new location, the control module may be docked in a fixed unit at the 40 new location and control by a central computer resumed.

The existing processing and display systems, described above, used in patient monitoring and treatment have numerous limitations. Such existing processing systems employ different software for monitor computers, anesthesia comput- 45 ers, ventilation computers, and fluid management computers. Further, system devices are typically transported and connected to a particular corresponding type of medical device computer (e.g., a monitor device may be transported and existing systems, medical device processing devices and displays are typically able to view and control parameters and functions of other like devices, that is, a monitor processing device and display is limited to be able to view and control parameters and functions of another monitor processing 55 device and display. In addition, existing systems typically derive patient parameters using specialized equipment and devices individually tailored to process a specific corresponding type of patient parameter. These devices require multiple individual electrical connections and fail to provide inter- 60 device communication and central parameter processing capability.

Consequently to provide a desired therapy to a patient, the patient monitoring and/or treatment modules required to provide that therapy is assembled at the patient bedside. They are 65 attached to the patient, and separately configured. Further, to provide the desired therapy may require changing the settings

of one of the patient treatment devices based on readings derived from another device, are required. Because the different patient monitoring and/or treatment modules are from different sources and include different user interfaces, there is a significant risk of a mistake being made in the settings of one device based on the readings from another. In order to minimize such mistakes, detailed instructions are provided to the clinician for operating the patient monitoring and/or treatment devices required to provide the desired therapy, and the requirement for human interaction with the patient monitoring and/or treatment modules slows the process of providing the desired therapy.

A wide variety of lung recruitment maneuvers are desirable respiratory therapies in the event of acute restrictive lung failure. It can be therapeutically beneficial, especially at an early stage, to reventilate lung areas which have collapsed in the course of the illness by inflating them with an applied pressure or volume over an adequate period of time. Following such a maneuver, the lungs need to be stabilized with an adequate positive end expiratory airway pressure (PEEP). The PEEP required for this is identified by measures such as an expiratory low flow maneuver or a slow step-by-step reduction in PEEP until the first manifestation of a so-called derecruitment—that is, a disproportionately high decrease in volume relative to the reduced pressure.

Therapeutic limitations, both in recruitment maneuvers and in maneuvers to determine the ideal ventilation settings, are typically the high pressures exerted over a long period of time on the chest cavity which reduce the venous return flow to the right heart and thus the cardiac output and the arterial pressure. As a countermeasure, a patient may be provided with an additional volume of circulating blood, in an effort to maintain an appropriate cardiac output and provide an adequate degree of blood flow (i.e., perfusion) to important tissues. However, the additional volume of circulating blood may result in the negative effect of increasing the intrathoracal pressure in the patient's chest cavity. Furthermore, if the pressure is suddenly and drastically reduced, the blood volume suddenly flowing back out of the capacity vessels (i.e., veins) into the right heart may overstrain the heart, particularly in patients with a coronary heart condition. If there is an insufficiency of the left heart, excessive volume input can lead to lung edema. A system according to invention principles addresses these deficiencies and related problems.

BRIEF SUMMARY OF THE INVENTION

In accordance with principles of the present invention, a connected to a corresponding monitor computer). Further, in 50 method and system for managing patient ventilator operation. A patient monitoring module receives data representing one or more hemodynamic parameters. A central processor, in response to the received data representing one or more hemodynamic parameters, provides one or more commands for adaptively altering ventilator operation. A patient treatment module provides signals for adaptively altering ventilator operation in response to the one or more commands from the central processor.

BRIEF DESCRIPTION OF THE DRAWING

In the drawings:

FIG. 1 is a block diagram of a prior art hospital system for monitoring patients and providing treatment to patients; and

FIG. 2 is a block diagram of a hospital system for monitoring patients and providing treatment to patients according to principles of the present invention;

FIG. 3 is a more detailed block diagram illustrating the interconnections of the central processor and the patient monitoring and treatment modules:

FIG. 4 is a more detailed block diagram of a central unit illustrated in FIG. 3;

FIG. **5** is a diagram illustrating the relationship between different components of the software controlling the central unit:

FIG. 6 is a flow diagram illustrating steps performed by an embodiment according to invention principles.

DETAILED DESCRIPTION OF THE INVENTION

FIG. 2 is a block diagram of a hospital system 200 for monitoring and providing treatment to patients. In FIG. 2, the 15 same four rooms are illustrated as are illustrated in FIG. 1, and those rooms contain the same medical equipment. The operating room 202 includes a patient monitoring module 210 for acquiring and processing signals derived from sensors (not shown) suitable for attachment to a patient. The operating 20 room 202 also includes patient treatment modules: a fluid infusion (IV pump) control and management module 212 and an anesthesia module 214. These modules (210, 212 and 214) are coupled to a central processor 220 via a patient area network (PAN) 216. The central processor 220 is coupled to 25 a display generator 222 which is coupled to a display device 223. The display generator 222 is also optionally coupled to a slave display device 224, as illustrated in phantom. The ICU room 204 includes a monitor module, a fluid management patient treatment module and a ventilator module, coupled to 30 a central processor via a PAN. The emergency room 206 includes a monitor module and a ventilator patient treatment module coupled to a central processor via a PAN. The other critical care room 208 includes a ventilator patient treatment module coupled to the central computer via a PAN 216.

In operation, the PAN 216 may be implemented in any manner allowing a plurality of modules to intercommunicate. For example, the PAN 216 may be implemented as an Ethernet network, either wired or wireless (WLAN). If implemented as a wireless network, it may be implemented according to available standards, such as: (a) a WLAN 802.11b compatible standard, (b) 802.11a compatible standard, (c) 802.11g compatible standard, (d) Bluetooth 802.15 compatible standard, and/or (e) GSM/GPRS compatible standard communication network.

The patient monitoring module 210 corresponds to the operational portion of a prior art patient monitor described above. It receives signals from the electrodes and sensors attached to the patient, performs the signal processing required to calculate the physiological parameters, and pro- 50 vides that information to the central processor 220 via the PAN 216. Similarly, the patient treatment modules, i.e. the fluid management module 212 and the anesthesia module 214, correspond to the operational portion of the prior art treatment modules described above. The patient treatment 55 modules 212, 214 receive operational data from the central processor 220 via the PAN 216 and in response perform their treatment functions, e.g. monitoring fluids administered to the patient and supplying anesthesia to the patient, respectively. Concurrently, the patient treatment modules 212, 214 60 send status data to the central processor 220 via the PAN 216. The central processor 220 processes the signals received from the patient monitoring module 210 and the patient treatment modules 212 and 214.

The central processor **220** interacts with the user to receive 65 patient identifier information and treatment instructions and parameters. The central processor **220** configures the patient

6

treatment modules 212, 214 by sending patient identifier information, the treatment instructions and parameters to the patient treatment modules 212 and 214 via the PAN 216.

The patient monitoring and/or treatment modules 210, 212, 214 may include a processor for receiving the configuration parameters from the central processor 220, for controlling the operation of the module 210, 212, 214 and for sending status and patient physiological parameter information to the central processor 220 via the PAN 216. The configuration parameters may include patient identifier information, set-up parameters, and/or data representing executable instructions for execution by the processor in the module 210, 212, 214 in processing data to be provided to the central processor 220. The modules 210, 212, 214, in turn, use the received configuration parameters, and executable instructions in supporting their operation, e.g. for processing data to be provided to the central processor 220.

As described above, there may be more than one central processor 220 in remote locations in the hospital. If a module 210, 212, 214 is disconnected from one central processor 220, then the patient identifier information, the set-up parameters and/or the executable instructions previously sent to it are used to control the operation of that module 210, 212, 214 while it is disconnected. If the disconnected module 210, 212, 214 is reconnected to a central processor 220, possibly in a different location than the central processor 220 from which it is disconnected, then the reconnected module 210, 212, 214 sends data representing the patient identifier information, the operational characteristics of the module, and any patient physiological parameter data gathered while disconnected to the central processor 220 to which it is connected.

The central processor 220 also receives signals representing physiological parameters from the patient monitoring module 210 and possibly from the patient treatment modules 212, 214. These parameters may be relatively standard physiological parameter, such as EKG, heart rate, SpO₂, etc. The central processor 220 may also initiate generation of a new parameter based on signals derived using the patient monitoring module 210 and/or the patient treatment modules 212, 214. For example, the new parameter may be associated with (a) gas exchange, (b) skin color, (c) haemodynamics, (d) pain and/or (e) electro-physiology.

The central processor 220 conditions the display generator 222 to generate signals representing an image for displaying 45 these physiological parameters in an appropriate manner, e.g. a waveform, a status phrase or a number. The display generator 222 is coupled to the display device 223 which displays this image. The display generator 222 may optionally send appropriate image representative signals to the slave display device 224. The slave display device 224 may have a larger, higher resolution screen, or may simply be a display device at a location remote from the location of the central processor. The image generated by the display device 223, under the control of the central processor 220 and display generator 222, may also integrate the display of patient identification, treatment instructions and parameters and status from the patient treatment modules 212, 214 in an appropriate manner. In this manner, information from users as well as patient monitoring modules 210 and patient treatment modules 212, 214 may be integrated into one or more composite images displayed on display devices 223 and 224, for example.

The central processor 220 may also communicate with the central processors of corresponding processing device and display systems in other locations in the hospital, such as those in the ICU room 204, the emergency room 206 and the other critical care room 208 via the critical care area network 205. The central processor 220 may optionally communicate

with a central hospital location via a hospital network 230, illustrated in phantom in FIG. 2. In this manner, patient physiological parameters and treatment instructions, parameters and status may be transmitted to a central location and stored in a central storage device 232, also illustrated in phantom.

FIG. 2 illustrates a patient monitoring module 210, and patient treatment modules for fluid management 212, anesthesia control 214, and ventilation control. However, one skilled in the art will understand that there are other monitoring and treatment devices which may include patient treatment modules for control and communication, such as: (a) an incubator, (b) a defibrillator, (c) a warming module, (d) a diagnostic imaging module, (e) a photo-therapy module, (f) a fluid input support module, (g) a fluid output support module, (h) a heart-lung support module, (i) a blood gas monitor, (j) a controllable implanted therapy module, (k) a controllable surgical table and weighing scale, and so forth. Modules for command and communication related to these and other patient treatment devices may be used as illustrated in FIG. 2.

FIG. 3 is a more detailed block diagram illustrating the system illustrated in FIG. 2. In FIG. 3, those elements which are the same as illustrated in FIG. 2 are designated by the same reference number and are not discussed in detail below. FIG. 3 illustrates the system as it would be implemented in one of the rooms 202, 204, 206 or 208 of FIG. 2. In FIG. 3, the central processor 220 and the display generator 222 are comprised within a central unit 300. The central unit 300 is a housing containing the circuitry and connectors necessary to interconnect the central processor 220 and the display generator 222 with: the patient monitoring and patient treatment modules 210, 212, 214, 250 and 260; the display devices 224, 320 and 330; and the multi-patient LAN 205 and hospital LAN 230.

The central processor **220** is coupled to a communications and power hub 235. The communications and power hub 235 35 comprises the patient area network (PAN) 216 and also a set 240 of module connectors coupled to the PAN 216: e.g. a patient monitor connector 241, a ventilator connector 243, a fluid management hub connector 245, an anesthesia delivery system connector 247 and a fluid (IV pump) management 40 connector 249. The connectors 240 permit the individual modules 210, 212, 214, 250, 260 to be plugged into and removed from the central unit 300 as required. In one embodiment, a user may activate a single mechanical release mechanism to remove a module 210, 212, 214, 250, 260 from the 45 central unit 300 or reattach a module to the central unit 300. The connectors 240 pass data signals between the modules 210, 212, 214, 250, 260 and the central processor 220 via the PAN 216.

The communications and power hub 235 further comprises 50 a power bus 234 for distributing power to the central unit 300. The power bus 234 is further coupled to the PAN 216 for receiving commands from and returning status to the central processor 220. The power bus 234 is also coupled to the connectors 240 (not shown to simplify the figure) to distribute 55 power to the patient monitoring and/or treatment modules 210, 212, 214, 250, 260. In this manner, the central processor 220 may manage the power-on and power-off status of the patient monitoring and treatment modules 210, 212, 214, 250, 260 in accordance with a set of predetermined rules maintained in the central processor 220.

As described above, at least some of the attached modules 210, 212, 214, 250, 260 include circuitry, e.g. batteries, which permit them to continue to operate when disconnected from the central unit 300. When docked, the central processor 220 65 conditions these modules 210, 212, 214, 250, 260 to transition from operating on battery power to operating on the

8

power supplied by the power bus 234 and recharge their batteries. The internal power supply circuitry of these modules 210, 212, 214, 250, 260 may also supply power supply status information, e.g. current battery capacity, to the central processor 220 through the connectors 240 and PAN 216. The central processor 220 may condition the display generator 222 to generate signals representing an image showing the battery charging condition of the patient monitoring and treatment modules 210, 212, 214, 250, 260 plugged into the central unit 300. This image may be displayed on the display devices 321, 331 and/or 225 in the main control panel 320, slave control panel 330 and/or remote display device 224, respectively.

As described above, the PAN 216 may be implemented as a wireless network. In such an embodiment, the central processor 220 may include a wireless communication interface to the PAN 216. Such an interface enables bidirectional communication with the patient monitoring and treatment modules 210, 212, 214, 250, 260 when they are disconnected from the central unit 300. This communications link enables the central processor 300 to maintain control of the patient monitoring and treatment modules 210, 212, 214, 250, 260 while they are disconnected from the central unit.

Individual patient monitoring and/or treatment modules 210, 212, 214, 250, 260 are coupled to corresponding ones of the connectors 240. For example, a patient monitor module 210 may be plugged into the monitor connector 241, a ventilator module 250 may be plugged into the ventilator connector 243, and so forth. The central unit 300 may include connectors 241, 243, 245, 247, 249 which are specific to the type of patient monitoring or treatment module, 210, 212, 214, 250, 260, expected to be plugged in. Alternatively, the modules 210, 212, 214, 250, 260 may be fabricated with the same type of connector and the connectors 240 may be the same type of matching connectors. In the former embodiment, a particular type of patient monitoring or treatment module 210, 212, 214, 250, 260 may be plugged into a connector 241, 243, 245, 247, 248 corresponding to that type of module. In the latter embodiment, any patient monitoring or treatment module 210, 212, 214, 250, 260 may be interchangeably plugged into any of the connectors 241, 243, 245, 247, 248.

As described above, the patient monitor module 210, plugged into the monitor connector 241, connects to a plurality of electrodes and sensors which may be placed on a patient. A monitoring pod 211 is used to connect the patientconnected electrodes to the patient monitor module 210. Similarly a ventilator module 250 may be plugged into the ventilator connector 243. The ventilator module 250, in turn, is coupled to a blower 254 and a humidifier 252. A fluid management hub 260 is plugged into the fluid management hub connector 245. Two fluid (IV pump) management modules 264 and 266 are plugged into the fluid management hub 267. Each fluid (IV pump) management module, 264, 266, is connected to an IV pump (not shown). An anesthesia delivery module is plugged into an anesthesia delivery connector 247. The anesthesia delivery module 214 is connected to a anesthesia delivery device (not shown). An individual IV pump 212 is coupled to an IV pump connector 249. Similar to the other IV pump modules 264 and 266, the fluid (IV pump) management module 212 is connected to an IV pump (not shown)

The central processor 220 is also coupled to the critical care area LAN 205, which, as illustrated in FIG. 2, is coupled to other central units 300 in processing device and display systems in other rooms. The central processor 220 may also be optionally coupled to a hospital LAN 230. The critical care

10 treatment modules 210, 212, 214, 250, 260 which are currently plugged into the central unit 300.

LAN 205 requires real time bandwidth quality-of-service while the hospital LAN 230 requires standard office bandwidth quality-of-service. As described above, if connected to a hospital LAN 230, the central processor 220 may exchange data with a central storage device 232, or any other desired device (not shown) at a remote location in the hospital. Data may be sent from patient monitoring and/or treatment modules 210, 212, 214, 250, 260 to the central storage device 232 through the connectors 240 to the central storage device 232 via the PAN 216 and from there to the central storage device 232 via the hospital LAN 230. In addition, control data may be sent in the other direction from the central location to a patient monitoring or treatment module 210, 212, 214, 250, 260.

It is further possible that a central processor 220 in a central 15 unit 300 in a processing device and display system in one treatment room 202, 204, 206, 208 may communicate with a second central processor 220 in a central unit 300 in a processing device and display system in a different treatment room 202, 204, 206, 208 (FIG. 2) via the critical care area 20 LAN 205 or the hospital LAN 230. In this manner, the central processor 220 in one treatment room may control the operation of the second central processor 220 in the second treatment room; may display patient related data received from the second central unit 300 in the different treatment room; and/ 25 or may send (a) a patient identifier identifying a particular patient and/or (b) medical information related to the particular patient to the second central processor 220 in the central unit 300 in the second treatment room 202, 204, 206, 208, which receives this information.

It is also possible for the central processor 220 to receive data from one or more of the patient monitoring and/or treatment modules 210, 212, 214, 250, 260, process that data and send control data to one or more of the patient treatment modules 212, 214, 250, 260 in response to the received data, 35 in a manner to be described in more detail below.

The display generator 222 is coupled to a main control panel 320. The main control panel 320 includes a display device 321, a keyboard 322 and a pointing device in the form of a mouse 324. Other input/output devices (not shown) may 40 be fabricated on the main control panel 320, such as: buttons, switches, dials, or touch screens; lights, LCDs, or LEDs; buzzers, bells or other sound making devices, etc. These input/output devices receive signals from and supply signals to the central processor 220, either through the display gen- 45 erator 222, or through separate signal paths, not shown to simplify the figure. The main control panel 320 may be fabricated as a part of the central unit 300, or may be fabricated as a separate unit. The display generator 222 is optionally coupled to a slave control panel 330, which substantially 50 duplicates the functionality of the main control panel 320, but is located remote from the central unit 300. The display generator 222 is also optionally coupled to a slave display device **224**. The slave display device **224** includes a display device 225, but does not include any of the other input/output devices 55 included in the main control panel 320 and slave control panel

In operation, the central unit 300 and main control panel 320 provide control and display functions for the patient monitoring and/or treatment modules 210, 212, 214, 250, 260 60 which are plugged into the common unit 300. A user may manipulate the input devices coupled to the main control panel 320, or slave control panel 330 if available, e.g. the keyboard 322, mouse 324 or other input devices described above. The resulting signals are received by the central processor 220. In response, the central processor 220 sends control signals via the PAN 216 to the patient monitoring or

Concurrently, the central processor 220 receives data signals from the patient monitoring and/or treatment modules 210, 212, 214, 250, 260, as described above, and conditions the display generator 222 to produce a signal representing an image for displaying the data from the patient monitoring and/or treatment modules 210, 212, 214, 250, 260, in an appropriate manner. For example, if a patient monitor 210 having the capability of performing an EKG on a patient is plugged into the central unit 300, EKG lead data from the patient monitor 210 is supplied to the central processor 220 through the monitor connector 241 via the PAN 216. The central processor 220, in turn, conditions the display generator 222 to produce signals representing an image of the EKG lead signal waveforms. These image representative signals are supplied to the display device 321 in the main control panel 320, which displays the image of the waveforms of the EKG lead signals. An image representing the heart rate of the patient, derived from the EKG lead signals, may also be similarly displayed in numeric form. Images representing other physiological parameters measured by the patient monitor 210, e.g. blood pressure, temperature, SpO2, etc. may also be displayed, in an appropriate form, on the display device 321 of the main control panel 320 in a similar manner. The image data may also be displayed on the display device 331 of the slave control panel 330 and on the display device 225 of the slave display 224, if they are available.

In a similar manner, images representing data received from the patient treatment modules, 212, 214, 250, 260, may be displayed on the display devices 321, 331, 225 in an appropriate form. Such data may represent, for example, present settings for the respective treatment modules, such as specified drip rates for IV pumps attached to fluid management modules 212, 264, 266. This data may be represented by images of appropriate form. Such data may also represent physiological parameters which may be measured by the patient treatment devices 212, 214, 250, 260. For example, respiration loops may be displayed in graphical form based on data received from the ventilator module 250, or drip rates for attached IV pumps may be displayed in numerical form based on data received from the fluid management hub 260.

A user may select which physiological parameters to display on the display device 321 and may arrange the location on the display device 321 of the images displaying the selected physiological parameters. In addition, the user may select different physiological parameters to display on the display device 321 in the main control panel 320 than on the display device 331 in the slave control panel 330 and/or on the display device 225 in the slave display 224. Further, the slave display device 224 may have a display device 225 which is larger and/or higher resolution than those in the main control panel 320 and the slave control panel 330, so that the images may be more easily seen, and/or may be displayed at an increased resolution.

The central processor 220 may also receive data from the power bus 234 via the PAN 216 representing the state of the power supplies in the patient monitoring and treatment modules 210, 212, 214, 250, 260. The central processor 220 may, for example, condition the display generator 222 to generate a signal representing an image representing the current charge condition of the respective batteries in the patient monitoring and treatment modules 210, 212, 214, 250, 260 plugged into the central unit 300, either separately or in composite, based on data received from the power bus 234. Further, the patient monitoring and/or treatment modules 210, 212, 214, 250, 260 may provide data to the central processor 220 indicating an

error condition in the module. The central processor 220 may condition the display generator 222 to generate a signal representing an image showing the user the error condition of that module.

The central processor 220 may also produce signals for controlling the operation of the other output devices on the main and slave control panel 320, 330, described above. For example, the central processor 220 may analyze the physiological parameters derived from signals received from the patient monitoring and/or treatment modules 210, 212, 214, 250, 260 to determine if any limits have been exceeded. This may entail separately calculating and verifying each physiological parameter response determined from a patient monitoring and/or treatment module, and comparing it to a predetermined parameter range to determine if it exceeds a limit, or analyzing more than one physiological parameter to determine if a function of those physiological parameters exceeds a limit. If a limit has been exceeded, then the central processor 220 may condition the output devices on the main and slave 20 control panel 320, 330 to provide an alarm. For example, the central processor 220 may generate a signal which activates a light, a buzzer, a bell and/or other such device on the main control panel 320, and/or the slave control panel 330, if available, to produce a visible or an audible alarm. The central 25 computer 220 may also send a signal over the critical care area LAN 205 and/or the hospital LAN 230 indicating that a limit has been exceeded. A similar alarm may be generated at the remote location in response to the receipt of this signal.

FIG. 4 is a more detailed block diagram of a central unit 300 illustrated in FIG. 3. In FIG. 4, those elements which are the same as those illustrated in FIG. 3 are designated by the same reference numbers and are not described in detail below. In FIG. 4, the central unit 300 is implemented on a computer system similar to typical personal computers. In such systems, a central processing unit (CPU) 402 controls the operation of the remainder of the system. The other elements illustrated in the central unit 300 are coupled to the CPU 402, though the connections are not shown to simplify the figure.

In FIG. 4, a power supply 450 provides power to the central 40 unit 300. The power supply 450 may be coupled to the power mains. The power supply 450 may also include batteries to provide power to the central unit 300. The batteries may operate in an emergency backup mode, in which if a power failure occurs at the power mains the battery is switched to supply power to the central unit. Alternatively, batteries may provide main power to the central unit, and the power mains used to maintain the battery at full charge, or to recharge the battery after a power failure. One skilled in the art will understand that other arrangements for supplying power to the 50 central unit 300 are possible.

A first Ethernet adapter 404 couples the CPU 402 to the patient area network (PAN) 216, which in turn is interconnected with patient monitoring and/or treatment modules 210, 212, 214, 250, 260. A second Ethernet adapter 406 55 couples the CPU 402 to the critical care area LAN 205. A third Ethernet adapter 432 couples the CPU 402 to the hospital LAN 230 which in turn is interconnected with the central storage device 232.

The display generator 222 couples the CPU 402 to the 60 display devices 321, 331 and 225 in the main control panel 320, the slave control panel 330 and the slave display 224, respectively. A set of panel I/O ports 410 couple the CPU 402 to the panel I/O devices, described above, on the main control panel 320 and the slave control panel 330. As previously 65 described, such I/O devices may include rotary switches, touch panels, pushbutton keys, lights, and so forth.

12

A watchdog circuit 430 checks the proper operation of the CPU 402 and produces a signal indicating a fault condition if the CPU 402 is not operating properly. The watchdog circuit 430 may check for proper operation of the CPU 402 using any of a variety of methods. For example, the watchdog circuit 430 may send a challenge signal at regular intervals to the CPU 402. If the CPU 402 is operating properly, it receives and recognizes the challenge signal, and provides a reply signal back to the watchdog circuit 430. If the watchdog circuit 430 does not receive the reply signal back from the CPU 402 within a specified time of issuing the challenge signal, then it detects a fault in the CPU 402, and produces the fault condition signal. The watchdog circuit 430 may also attempt to restart operation, i.e. reboot of the CPU 402, upon detecting a fault in the operation of the CPU 402.

The remainder of the elements illustrated in the central unit 300 are typically included in personal computers. A keyboard/mouse interface 408, typically using a PS/2 or USB standard, couples the keyboard 332 and mouse 324 to the CPU 402. A sound card 412 responds to instructions from the CPU 402 to generate sound representative signals, which may be coupled to speakers (not shown) to reproduce sound. A read-write memory unit (RAM) 414 provides local storage for programs controlling the CPU 402 and for data used and/or created by the CPU 402. A serial port 416 exchanges serial binary data signals with external peripherals e.g. using the RS232 standard. A USB port 418 similarly exchanges serial binary data signals with external peripherals using the USB standard. A DVD/CD player 420 allows the CPU 402 to access data on DVDs and/or CDs. It is also possible to write data onto DVDs and/or CDs. An expansion card port 422 allows the CPU to exchange data with portable devices, such as a Personal Computer Memory Card International Association (PCMCIA) card, Compact Flash (CF), Secure Digital (SD), and so forth. A real time clock (RTC) 424 with its associated battery 425, maintains and provides current time and date to the CPU 402. An integrated drive electronics (IDE) bus 426, into which conforming cards may be plugged, allow such cards to exchange information with the CPU 402. Similarly, a peripheral component interconnect (PCI) bus, into which conforming cards may be plugged, allow such cards to exchange information with the CPU 402. Cards plugged into either the IDE bus 426 or the PCI bus 428 may be coupled to peripheral devices, both internal and external to the central unit 300, and permit the CPU 402 to exchange data with the peripheral devices.

In operation, the CPU 402 interacts with the peripheral devices connected to it under control of software. Because the central unit 300 is designed and implemented similarly to a typical personal computer, it may be controlled using software typically executed on a personal computer, augmented by executable applications for performing specialized tasks related to monitoring and providing treatment to patients.

FIG. 5 illustrates the relationship and interaction among different components of the central unit 300, including both the hardware platform 504 (as illustrated in FIG. 3 and FIG. 4) and a system executable application 500. As described above, an executable application is any set of executable instructions, code or machine readable instructions for controlling the operation of a programmable processor or conditioning a processor to implement predetermined functions, such as those of an operating system, a context acquisition system or other information processing system, for example, in response to user command or input. It may include software, firmware and hardware, as appropriate, and one skilled in the art will understand how to partition the executable application into software, firmware and hardware, and the design criteria

and tradeoffs involved. Because, as described above, the components illustrated in FIG. 5 are implemented on a hardware system based on available PC systems, the executable application described in FIG. 5 is implemented in software, and will be termed system software 500 below.

A user interface (UI), as used herein, comprises one or more display images, generated by a display processor and enabling user interaction with a processor or other device and associated data acquisition and processing functions. The UI also includes an executable procedure or executable applica- 10 tion. The executable procedure or executable application conditions the display processor to generate signals representing the UI display images. These signals are supplied to a display device which displays the image for viewing by the user. The executable procedure or executable application further 15 receives signals from user input devices, such as a keyboard, mouse, light pen, touch screen or any other means allowing a user to provide data to a processor. The processor, under control of an executable procedure or executable application manipulates the UI display images in response to the signals 20 received from the input devices. In this way, the user interacts with the display image using the input devices, enabling user interaction with the processor or other device. The functions and process steps herein may be performed automatically or wholly or partially in response to user command. A document 25 human interface component 512 (see Table 1 (below)). The or record comprises a compilation of data in electronic or paper form.

Each element in FIG. 5 is represented by a rectangle. In general, elements, and the functions they provide, at lower levels of FIG. 5 may be accessed by elements at higher levels. 30 At the bottom of FIG. 5 is the hardware platform 504. The hardware platform 504 provides the hardware functions, described in more detail above, such as: providing control signals to, and receiving status and patient physiological parameter information from, patient monitoring and/or treat-35 ment devices 210, 212, 214, 250, 260; exchanging data over the critical care area LAN 205 and hospital LAN 230; providing image representative signals to display devices 222, 225, 321, 331 (FIG. 3), exchanging signals with panel I/O devices 410 (FIG. 4), and so forth. The hardware platform 504 40 is not part of the system software 500 illustrated by the remainder of FIG. 5.

The system software 500 illustrated in FIG. 5 includes a software framework 502 providing particular functions. The software framework 502 provides the software infrastructure 45 for support of point of care based medical modules, such as the modules 210, 212, 214, 250, 260 (FIG. 2, FIG. 3, FIG. 4). As used herein, the point of care (POC) is the area, in the vicinity of the patient, in which medical treatment is provided to a patient. The software illustrated in FIG. 5 may be embod- 50 ied in PC based products. Table 1 (below), describes in detail the functions provided by the respective software components illustrated in FIG. 5.

The software framework 502 includes a hardware dependent operating system 506, which in FIG. 5 is an embedded 55 windows operating system (OS) 506. For example, an embedded version of Windows XP (by Microsoft Corp) OS 506 may be included in the software framework 502. The OS 506 interacts with the hardware 504, which may be different from product to product, or may change or be updated over time. 60 The OS 506 also provides a set of application program interfaces (APIs) which are sets of common software interfaces which may be used by the remainder of the software and which remain unchanged despite differences in the hardware **504**. The remainder of the software illustrated in FIG. **5** is 65 related to providing the functions required by the modules which may be controlled by the central unit 300.

14

The software framework 502 further includes a set of common platform components 508 (see Table 1 (below)). These components provide monitoring and executive functions for the central unit 300. Specifically, a watchdog function, a resource monitor, and a monitor for critical components are provided by the common platform components 508. In addition, the common platform components 508 provide security. lifetime management, diagnostics, real time infrastructure and event management, safety and availability management, and user set up configuration support for the central unit 300.

The software framework 502 also provides common communications component 510 (see Table 1 (below)). More specifically, the common communications component provides access to the PAN 216, the critical care area network 205 and any other networks to which the central unit 300 may be coupled, such as the hospital network 230 (FIG. 3). The common communications component 510 also provides peripheral support, e.g. communications with any other auxiliary device via the serial port, 416, the USB port 418, the expansion card port 422 and/or any other device which may be coupled to the central unit 300, for example, via boards mounted in the IDE bus 426 or PCI bus 428.

The software framework 502 also provides a common common human interface component 512 provides functions for displaying graphical user interfaces (GUIs) on display devices 225, 321, 331 (FIG. 3, FIG. 4) and for coordinating the user inputs received from the input devices, such as keyboard 322 and mouse 324, with the displayed GUI. This enables a user to control the configuration and operation of the system and to receive status and data representing patient physiological parameters from the system. These functions also provide parameter signal group support, deployment support, and user help.

These functions also include those GUI functions which are specific to a patient monitoring and treatment module, for example, support for the display of waveforms, such as EKG waveforms or respirator loops, maintenance of trends, and generation of reports. These GUI functions also include the ability for a user to arrange on the screen of the display device the images representing the physiological parameters of the patient. That is, to be able to move those images around on the screen, to resize them, to remove an image displaying a physiological parameter and/or to insert an image displaying a different physiological parameter. The common human interface 512 further supports maintenance of patient data and status, and the database containing these and/or other data items. The common human interface 512 component further provides alarm support and processing, including providing functions for generating an audible and/or visible alarm at the central unit 300 (FIG. 3, FIG. 4), and for transmitting alarm information to other locations, via the PAN 216, the critical care area network 205 and/or the hospital network 230. The common human interface component 512 also provides more standard GUI support for other software applications (described in more detail below), which may not be related directly to medical support.

The remainder of the components in the system software are application programs 520. An application program is software which uses functions provided by the software framework **502**, described above, to support clinical domains and/or to provide clinical functions at the point of care. As used herein, a clinical domain is an area of a patient monitoring and/or treatment process. For example, patient monitoring is a clinical domain; patient ventilation is another clinical

domain; anesthesia and fluid administration are others, and so forth. The system software 500 includes several types of application programs 520.

The application programs **520** include a set of common point of care (POC) applications **522** (CPOC) which are 5 common to the clinical domains (see Table 1 (below)). The functions provided by the CPOC **522** are application-related but generic and not specific to any particular domain. That is, the central processor **402** in the central unit **300** executes at least a portion of the common code in the CPOC application 10 **522** to support the operation of two or more of the patient monitoring and/or treatment modules **210**, **212**, **214**, **250**, **260**

For example, the CPOC application 522 may provide a home screen from which other functions may be selected and 15 configured. Functions for configuring and controlling the central unit 300 itself may be selected from the home screen, including: software option handling; application selection and configuration; remote control, both wired and wireless, from e.g. slave control units (FIG. 4: 330) or other central 20 units via the critical care area network 205 and/or the hospital area network 230 (FIG. 2); battery management; and so forth. In addition, functions related to patients may be selected from the home screen, including patient category, configuration, context, setup and demographic entry, editing, and transfer. 25 The CPOC application 522 may also provide functions related to monitoring and/or treating patients, including: realtime processing of measurements, waveform display; alarm behavior, display and control; measurement setup and priority, events, trends, strip recordings; loop display; flow meter 30 display; alarm limits and history, and so forth.

One skilled in the art will recognize that point of care (POC) patient monitoring and/or treatment modules, e.g. 210, 212, 214, 250, 260 (FIG. 3 and FIG. 4), are typically associated with a specific clinical domain. That is, the monitoring 35 module 210 is associated with the patient monitoring domain; the anesthesia module 214 is associated with the anesthesia domain, and so forth. Specific POC applications (SPOC), of which three 523, 524, 526 are shown to simplify the figure, respectively correspond to POC modules for specific domain 40 areas. The respective SPOC applications 523, 524, 526 interact with associated ones of the modules 210, 212, 214, 250, 260. For example, in FIG. 5, SPOC 523 may be associated with one type of POC module, e.g. anesthesia module 214; SPOC 524 may be associated with a different type of POC 45 module, e.g. fluid management module 212; and SPOC 526 may be associated with another POC module, e.g. patient monitoring module 210.

Typically, SPOC applications 523, 524, 526 have a presentation function e.g. 523A, a control and management function 50 e.g. 523B, a data server function e.g. 523C, and a pluggable front-end (FE) module interface function e.g. 523D. As used herein, the term pluggable front end module refers to a medical monitoring and/or treatment module, such as modules 210, 212, 214, 250, 260 (FIG. 2, FIG. 3 and FIG. 4), which 55 may be connected to and disconnected from the central unit 300 during operation. The FE module interface function e.g. **523**D, bidirectionally communicates with patient monitoring and treatment modules 210, 212, 214, 250, 260. These communications include control and status information and 60 physiological parameter representative data. The data server function e.g. 523C makes the control status and physiological data available to other applications. The presentation function e.g. 523A makes the control, status and physiological data available to be displayed on the display devices 225, 321, 331 65 (FIG. 3). The control and management function e.g. 523B controls the operation of the SPOC and the FE module.

16

More specifically, the SPOC application **526**, which is associated with a patient monitoring module **210**, provides the specific functions required to control and interact with the monitoring module **210**. As described in more detail in Table 1 (below), the monitoring SPOC **526** provides module management, control and report functions, such as: monitor setup; export protocol management; nurse call; and setting display modes, including bedside and surgical display modes. The monitoring SPOC **526** also provides physiological parameter monitoring functions, such as: EEG, SpO₂, respiratory mechanics, invasive and non-invasive blood pressure, body temperature, transcutaneous blood gases, and so forth.

The SPOC application 523, which is associated with the anesthesia module 214, provides the specific functions required to interact with the anesthesia module 214. As described in more detail in Table 1 (below), the anesthesia SPOC 523 provides module management, control and report functions such as: warm up; carrier gas selection, and so forth. The anesthesia SPOC 523 also provides anesthesia control and monitoring functions, such as anesthetic gas control, including N_2O , Xenon, etc.; consumption monitoring, and anesthetic gases supply, and so forth.

The SPOC application **524**, which is associated with the fluid management module **212**, provides the specific functions required to interact with the fluid management module **212**. As described in more detail in Table 1 (below), the fluid management SPOC **524** provides functions supporting different fluid managements modes, including: total controlled infusion (TCI), total intravenous anesthesia (TIVA), and patient controlled analgesia (PCA). As described above, other medical monitoring and/or treatment modules **210**, **212**, **214**, **250**, **260**, corresponding to other medical domains, are associated with SPOC applications which control and manage them. Details for these SPOCs are described in detail in Table 1 (below).

The application programs 520 further include cross domain POC applications (CDPOC), one of which 528 is shown in FIG. 5 to simplify the figure. CDPOC applications provide advanced integrated clinical information. This information may be derived from cooperative operation of two or more selected SPOC applications 523, 524, 526 controlling associated medical monitoring and/or treatment modules 210, 212, 214, 250, 260 in respectively different clinical domains such as monitoring, ventilation, anesthesia and/or fluid management. CDPOC applications coordinate the operation of the selected medical monitoring and/or treatment modules 210, 212, 214, 250, 260, and integrate data received from them, as described in more detail below. One skilled in the art will understand that other CDPOC applications may be included in the application programs 520 which coordinate different SPOC applications; that more than two SPOC applications may be coordinated by a CDPOC application, and that an SPOC application may be associated with more than one CDPOC application.

Referring specifically to FIG. 5, the CDPOC application 528 coordinates the operation of the fluid management SPOC 524 and the monitoring SPOC 526. The fluid management SPOC 524 controls the operation of a fluid management treatment module 212 which may be administering a medication to affect a particular patient physiological parameter, such as blood pressure. The monitoring SPOC 526 controls the operation of the patient monitoring module 210 to monitor the patient blood pressure, among other things. The CDPOC application 528 monitors the patient blood pressure, as reported by the monitoring SPOC application 526 and controls the fluid management SPOC application 524 to con-

tinually adjust the administration of the blood pressure medication to maintain the patient blood pressure within limits specified by the physician.

The application programs **520** may further include imaging applications **530**, as described in more detail in Table 1 (below). These applications condition the various display devices, **225**, **321**, **331** (FIG. 3) to display designated images in 2D and 3D modes. These imaging applications **530** further provide user control of panning and zooming, and for 3D images setting a point of view. The imaging applications **520** may also be used to produce: a virtual film sheet for e.g. x-rays, CAT scans, or any other group of related images; a patient scanner; a viewer for DICOM (Digital Imaging and Communications in Medicine) images retrieved via a query/retrieve operation, and so forth.

The application programs 520 may further include information technology (IT) applications 532, as described in more detail in Table 1 (below). Such applications may include e.g. a chart assistant program, a remote viewing program, and other programs for exchanging and analyzing information. 20 Other third party applications 534 may also be included in the application programs 520. As used herein, third party applications 534 may provide clinical functions which may provide a benefit at the point of care, and may be developed outside and independently of the architecture developed for 25 the central unit 300 to interact with the medical monitoring and/or treatment modules 210, 212, 214, 250, 260. For example, medical image and report distribution, appointment scheduling, client records management, copayment tracking and billing, medical charting, insurance submission and billing, scheduling, and so forth are functions which may be provided by third party application programs 534.

A Semantical Product Application (SPA) 536 provides coordination for the application programs 520 included in the system software. The SPA 536 covers the target domain or 35 domains of the system, as configured with selected medical monitoring and/or treatment modules 210, 212, 214, 250, 260. The SPA 536 uses, deploys and combines other application programs 520. More specifically, the SPA 536 includes SPOC 523, 524, 526 configuration; CPOC 522 configuration; 40 and CDPOC 528 configuration functions, and so forth. The SPA 536 also provides version management for the system.

The central units 300 in the respective critical areas and/or the hospital employ substantially the same type of CPU 402 and are implemented to support the operation of the different 45 types of patient monitoring and/or treatment modules 210, 212, 214, 250, 260. In addition, the central processor 220 in the respective central units 300 in the critical care area and/or the hospital employ substantially the same system software 500, described above, supporting the operation of the patient 50 monitoring and/or treatment modules 210, 212, 214, 250, 260.

The hardware and software architecture described above and illustrated in FIG. 2, FIG. 3, FIG. 4 and FIG. 5 allows implementers to develop different products which address a 55 desired medical domain or domains. As used herein, a product addresses the desired domains using the hardware and software architecture to provide a well defined set of applications for the target domains. That is a fabricator may produce a monitoring product by including a monitoring SPOC 60 (e.g. 526) and a patient monitoring module (e.g. 210). Alternatively, further capability may be included, such as including a ventilation SPOC (not shown) and a ventilation patient treatment module (also not shown), a fluid management SPOC (e.g. 524) and a fluid management patient treatment module (e.g. 2112), and an anesthesia SPOC (e.g. 523) and an anesthesia patient treatment module (e.g. 214). A CDPOC

18

(e.g. **528**) application may be added to coordinate the operation of two or more SPOC applications.

More specifically, a fabricator may implement a product such as a transportable breathing support equipment system. Such a device is illustrated in FIG. 2 in room 208. This system includes a central unit 300 (FIG. 3) (not shown) which incorporates a central processor 208B and docking connectors 240. A ventilator module 208A is coupled to the central processor 208B and a display device 208C via a PAN 208D. The ventilator module 208A controls a ventilator device (not shown) The ventilator device regulates the flow of breathable gas from a source (not shown) to the lungs of the patient. The ventilator module 208A includes at least one battery which powers the module 208A and the ventilator device itself during transportation. The docking connectors 240 allow other modules, such as a patient monitoring module 210, an anesthesia module 214 and/or a fluid management module 212, to be connected to the breathing support equipment system if desired. The system software 500 (FIG. 5) detects the presence of these modules and automatically loads the SPOC applications required to control the newly added modules, **210**, **212**, **214**, **250**, **260**. The transportable breathing support equipment system may comprise a manually pushed, or power driven cart or trolley conveying the equipment.

Other products such as an emergency room product as illustrated in room 206 (FIG. 2) and including a patient monitoring and ventilator module, or an ICU room product as illustrated in room 204 with a patient monitoring, ventilator and fluid management module, both with capabilities of adding further modules as required, may be implemented in a similar manner.

As described above, a CDPOC application 528 can advantageously coordinate the operation of two or more SPOC applications 523, 524, 526, which in turn control the operation of associated patient monitoring and/or treatment modules 210, 212, 214, 250, 260. This coordination enables the central processor 220 (FIG. 2) to support monitoring operation of a patient treatment module 212, 214, 250, 260 by (a) deriving data, based on combinations of parameters derived from the patient monitoring module 210 and a patient treatment modules 212, 214, 250, 260, for presentation to a user, and/or (b) prompting a user with suggested patient treatment module 212, 214, 250, 260 configuration settings.

The central processor 220 may also verify the safety of the treatment by receiving data from the patient monitoring and/ or treatment modules 210, 212, 214, 250, 260 and using said received data to determine whether settings of the treatment delivery devices attached to the patient treatment modules 212, 214, 250, 260 are compatible with the desired treatment to be delivered to a patient. That is, the central processor 220 may verify the safety of a desired treatment by comparing patient physiological parameters received following initiation of delivery of a treatment, or following a change in the treatment induced by a corresponding change in the settings of a patient treatment module 212, 214, 250, 260, with predetermined physiological parameter value response ranges. In response to a determination that the settings of a patient treatment module 212, 214, 250, 260 are incompatible with a desired treatment the central processor 220 may (a) automatically alter the settings and/or (b) initiate generation of an alert message to a user warning of the incompatibility.

This coordination among different patient monitoring and/ or treatment modules 210, 212, 214, 250, 260 allows patient medical tests to be performed, and physiological parameters to be determined, by such a system, without requiring the use of more expensive, or more invasive testing methods. A single configured system as illustrated in FIG. 4 and FIG. 5, for

example, advantageously automatically performs multiple different tests as described as follows. The tests in some instances may involve manual interaction. One skilled in the art will understand which patient monitoring and/or treatment modules to include in the system, how to coordinate the operation of these modules, and how to analyze the data from those modules to perform the desired medical tests.

A general form of such patient medical tests involves providing a predetermined physiological stimulus to a patient, monitoring the patient physiological parameters after the 10 stimulus, and verifying an acceptable response. For example, the physiological stimulus may be (a) a medication, (b) a gas administered to said patient, (c) an electrical stimulus, (d) a physical or mechanical stimulus, (e) an application of heat or cold, (f) an acoustic stimulus, (g) a light stimulus and/or (h) a 15 radiation stimulus. The patient physiological parameters monitored may be (a) BP, (b) HR, (c) RR, (d) SpO₂, (e) O₂, (f) CO₂, (g) NBP, (h) EEG and/or (i) blood gas parameters.

In the system described above, the central processor 220 (FIG. 4) may initiate a stimulus by conditioning a patient 20 treatment module 212, 250, 260 to temporarily change its operational setting, and using the patient monitoring module 210 to monitor subsequent physiological parameters to verify an acceptable response.

A more specific example of a medical test is a respiratory 25 systolic variation test (RSVT), which may be performed by such a system. This test determines the blood filling conditions in the left atrium. It enables a physician to manage fluid input and output of a patient, and lung recruitment efforts (hypovolemea is often the reason for a patient not tolerating pressure-controlled inverse ratio ventilation (PCIRV)). The result of this test is a patient physiological parameter which may be displayed on the display devices **225**, **321**, **331** (FIG. **3**). Use of the system described above to provide the RSVT test is more accurate and less invasive than the use of a single 35 use PA catheter, which at the present time costs around \$100.

A Gedeon non-invasive cardiac output test (NICO) may also be performed by the system described above. This test estimates output of the left ventricle and effective gas exchange area of the lungs (i.e. the effective lung volume 40 (ELV). It enables a physician to titrate the positive end-expiratory pressure (PEEP) for optimal CO and ELV after initiating mechanical ventilation. As used herein, the term "titrate" refers to the adjustment of a patient treatment parameter (such as the PEEP pressure) such that a desired patient 45 physiological parameter is achieved (that is, optimal CO and ELV). The titration may be performed manually by the physician in response to the results of the test, or may be performed automatically under the control of a CDPOC (not shown) programmed to perform the test and titrate the PEEP 50 parameter. The results of this test may be displayed on the display devices 225, 321, 331 (FIG. 3). This test also aids a physician in starting or monitoring inotropic (i.e. cardiac output enhancing) drug therapy. Use of the system described above to perform the NICO test is less invasive than the 55 conventional method and more accurate than other NICO

A lung mechanics calculation test (LMC) may also be performed by the system described above. This test permits the modeling of a patient respiratory system in terms of elastic 60 and resistive forces. More specifically, this test may determine inflection points in the respiratory cycle, i.e. points of alveolar collapse (atelectasis) during expiration and hyperinflation during inspiration. This test may also calculate physiological dead space, i.e. air which is inhaled by the body in 65 breathing, but which does not partake in gas exchange. The results of the former test may be numerical or a graphic

20

display, and the results of the latter test may be a numerical display, either or both of which may be displayed on the display devices 225, 321, 331 (FIG. 3). The physician may use the results of this test to titrate the settings after initiating mechanical ventilation, or a CDPOC may be programmed to titrate the settings automatically. The LMC test has been tested and widely published. It is considered state-of-the-art at this time for lung mechanics. The NICO test requirements, described above, may be combined with this test.

A stress index test (SI) may also be performed by the system described above. This test quantifies the stress on the lungs induced by mechanical ventilation. More specifically this test detects and measures the effect of cyclic stretch, i.e. recruitment of alveola at the extreme end of inspiration and collapse at the extreme end of expiration. The results of this test may be numeric or graphical and may be displayed on the display devices **225**, **321**, **331** (FIG. **3**). A physician may use the results of this test to titrate ventilator settings, such as PEEP and tidal volume (V_T) to reduce stress on the lungs during ventilation, or a CDPOC may be programmed to titrate the settings automatically. The results of this test may also be used to predict the probability of success of a lung recruitment attempt. Ventilator settings made according to the SI test have been proven to reduce inflammatory markers in lung tissue.

An automatic lung parameter estimator test (ALPE) may also be performed by the system described above. This test assists a physician in quantifying the amount of pulmonary shunt and the distribution of pulmonary circulation (e.g. ventilation-perfusion ratio (V/Q) scatter). This test may also detect and quantify cardiac congestion, i.e. congestive heart failure (CHF). The results of this test may be numeric or graphical and may be displayed on the display devices 225, 321, 331 (FIG. 3). A physician may use the results of this test to determine the use of diuretics and inotropic drugs to manage CHF. This test provides a comprehensive model of hemodynamic status and blood gasses non-invasively. This may be useful to a physician in the detection and management of CHF, which is a widespread disease, especially prevalent among respiratory patients.

Diaphragm electromyographically (EMG) controlled ventilation may also be advantageously performed by the system described above. In this ventilation mode the electrical signal related to the diaphragm muscle contraction is detected using electrodes on an oesphageal catheter. Because contraction of the diaphragm muscles occurs when a patient begins to take a breath, the EMG signal may be used to trigger the ventilator to begin a respiration cycle. Thus, this ventilation mode permits the patient's brain to advantageously control respiratory support. This mode may be selected by a user selection via the interaction of the GUI and user input devices such as the keyboard 322 and mouse 324, or by panel I/O devices on the main control panel 320 and/or slave control panel 330 (FIG. 3, FIG. 4). Using EMG signals to trigger respiration permits ventilation to be more closely matched to the patient. This enables support of spontaneous breathing for a wider range of patients. This, in turn, makes mask ventilation more feasible, reducing complications associated with intubation, such as nosocomial pneumonia. These electrical signals may also provide ECG signals to measure the posterior of the heart and potentially detect atrial arrhythmias. The results of an ECG using EMG signals may be displayed on the display devices 225, 321, 331 in graphical form. An alarm may also be sent if an arrhythmia is detected. Detection of cardiac ischemia and atrial arrhythmias permits earlier intervention.

Some patients have responded successfully in certain therapy phases to the maneuvers previously mentioned and such maneuvers are becoming increasingly popular. How-

ever, the inventors have recognized that a risk is posed by the inadequate consideration of hemodynamic and cardiac implications. It is advisable to monitor parameters associated with the mechanics of the patient's blood circulation (i.e., hemodynamic parameters) such as the arterial blood pressure or the cardiac output or both and to end or alter the maneuver if there is a significant change in the value(s) of the monitored parameter(s).

Various procedures, also known as ventilation maneuvers, that alter the operation of a device or apparatus that is providing mechanical ventilation to a patient, may also be performed by the system described above. One example of a ventilation maneuver is a lung recruitment maneuver to reexpand collapsed lung tissue. Types of lung recruitment 15 maneuvers may include, but are not limited to, regular sighs, sustained inflations, successively increased PEEP, and successively increased inspiratory pressure, or combinations thereof. A maneuver as used herein and in the claims comprises a procedure that provides signals that alters the opera-20 tion of a device or apparatus (e.g., ventilator) that is providing mechanical ventilation to a patient. A hemodynamic parameter as used herein and in the claims comprises a blood related parameter that may include, for example, cardiac output and blood pressure (of different types). A regular sighs lung 25 recruitment maneuver as used herein and in the claims comprises a controlled increase in the tidal volumes, PEEP or inspiratory pressure during a small number of successive assisted breaths produced at regular intervals. A sustained inflations lung recruitment maneuver as used herein and in the 30 claims comprises continuous elevated airway pressure (above PEEP) applied for a specified time, typically up to 40 seconds but sometimes longer. A successively increased PEEP lung recruitment maneuver as used herein and in the claims comprises progressively increasing PEEP with each breath, or 35 every few breaths, up to a maximum PEEP. A successively increased inspiratory pressure lung recruitment maneuver as used herein and in the claims comprises progressively increasing inspiratory pressure with each breath, or every few breaths, up to a maximum inspiratory pressure.

Another example of a ventilation maneuver is a low flow PV maneuver to determine appropriate ventilator settings. A low flow ventilation maneuver as used herein and in the claims comprises controlled inflation and deflation of a lung with a low constant flow in order to recruit the lung and 45 determine characteristics derived from the recorded elastic properties of the lung while keeping the flow as low and constant as possible.

In one embodiment of the present invention, while the system is executing a ventilation maneuver under the control 50 of the central processor 220 through a patient treatment module that is configured to control and communicate with the ventilator 250, the patient monitor 210 monitors the arterial blood pressure and/or the cardiac output. If one or both of these parameters fall below a respective threshold while the 55 pressure in the thorax is increasing, the maneuver is limited or aborted (i.e., terminated) by the central processor 220 and/or the central processor 220 provides an alarm. As used herein, limiting a maneuver refers to switching to low flow expiration while continuing the maneuver, and aborting a maneuver 60 refers to immediately relieving the airway pressure to the PEEP. As is well-known, there is a trade-off between aborting or limiting a maneuver. Aborting a maneuver has the benefit of providing a rapid relief of pressure in the thorax favoring a rapid restoration of the arterial pressure, while limiting a 65 maneuver has the competing benefit of not overstraining a possibly pre-damaged heart.

22

In one embodiment, a user configures the action (limit or abort) to be taken by the system when the parameter(s) fall below their respective thresholds. In another embodiment, the system also receives information regarding the ST segment from the patient monitor 210, and automatically determines the action (limit or abort) based on the amount that the arterial blood pressure and cardiac output parameter(s) have fallen and also on the ST segment information. As is well-known, a typical ECG waveform consists of a P wave, a QRS complex and a T-wave. The portion of the ECG waveform between the end of the QRS complex and the beginning of the T-wave is referred to as the "ST segment." It is also well-known that an elevated or depressed ST segment (relative to the baseline at the end of the QRS complex) may be an indication that the heart has been damaged. In such case, the maneuver should be gradually limited so as not to expose the heart to excessive preload due to the return flow of a large blood volume from the capacity vessels. FIG. 6 depicts steps that may be performed by such an embodiment of the present invention. In Step 1, the system starts the maneuver. The arterial blood pressure and cardiac output parameters are tested by the system as shown in Steps 2 and 3. If the arterial blood pressure falls more than X % or the cardiac output falls more than Y %, then the information regarding the ST segment is tested as shown in Step 4. If the ST segment information indicates possible heart damage, then the central processor 220 limits the maneuver as shown in Step 5. In some embodiments, the rate at which the maneuver is limited is based on the degree of estimated heart damage as indicated by the ST segment information. If the ST segment information does not indicate possible heart damage, then the fall in arterial pressure and cardiac output are again tested, as shown in Steps 6 and 7, against higher thresholds, Z % and A %, respectively, where Z>X and A>Y. If either of the higher thresholds is exceeded, then the central processor 220 aborts the maneuver as shown in Step 8. Otherwise, the maneuver is limited as shown in Step 5.

The thresholds for the fall in arterial blood pressure and cardiac output and the desired response (limit, abort and/or alarm) may be adjustable by a user, and may be assigned defaults, such as a 50% fall in arterial blood pressure and 60% fall in cardiac output. In some embodiments, either or both of the arterial blood pressure and cardiac output parameters are averaged and/or their deviations from previous baselines are integrated over time before comparing to the thresholds. In one such embodiment, averaging is performed over a time interval of duration such that a fall in parameter value can be recognized quickly, e.g., within a heartbeat.

In some embodiments, the system will slowly reduce pressure when limiting a maneuver, so as not to expose the heart to excessive preload due to the return flow of a large blood volume from the capacity vessels. For example, if the heart is in poor condition, as indicated by the ST parameter and/or additional information available to the central processor 220, then the pressure will be reduced slowly. Similarly, if the integrated value of the arterial blood pressure's deviation from a baseline over time is high, then the system will reduce the pressure more slowly.

One skilled in the art will understand that various devices that are capable of performing ventilation functions may be used in the system described above. For example, a ventilator may be used; similarly, a device that delivers anesthesia to the patient may also incorporate ventilation functions and thus may be suitable for use in the system.

The system described above may also be used to perform electrical impedance tomography (EIT). EIT may provide continuous, breath-to-breath, and beat-to-beat anatomical images of respiratory and cardiac dynamics and distribution,

respectively. More specifically, the physician may see and quantify areas of atelectasis and hyperinflation in the lungs and/or may see and quantify the output of the right ventricle and the deposition of blood in the lungs with each heartbeat. Electrodes for providing current and sensing voltage are 5 applied to the patient and appropriate signals are applied to them to sense the conductivity of the respective portions of the body. From these readings, an anatomical image, or realtime series of images, may be synthesized. The display generator 222 (FIG. 4) generates signals representing these 10 patient anatomical images. In order to maintain the display of these images in real time, the interface between the processor 402 and the display generator 222 provides substantially real time bidirectional communications. These images may be displayed on the display devices 321 and 331 on the main control panel 320 and slave control panel 330, respectively. These images may also be supplied to the larger display device 225 on the slave display panel 224. The physician may optimize ventilation parameters to address V/Q mismatch in which lung compartments are either ventilated but not per- 20 fused, or perfused but not ventilated. Early intervention, available from EIT images, may prevent cascade of lung injury leading to acute respiratory distress syndrome (ARDS) and sepsis. Use of EIT also has the possibility to reduce the number of CT and X-ray images required, and the intra- 25 hospital transport required for them.

Referring again to FIG. 5, the embedded operating system 506 is configured to monitor the input/output ports, which may include the serial port, 416, the USB port 418, the expansion card port 422, the Ethernet ports 404, 406, and/or the 30 panel I/O ports 410 to detect when a hardware device is newly connected to the system. When newly connected hardware is detected, at least the portion of the software required by the system software 500 to interact with this new hardware is retrieved from a mass memory, installed in the RAM 414 and 35 made available to the operating system 506 and the rest of the system software 500. This operation is sometimes called "plug-and-play". The mass storage device may be local to the central unit 300, or may be remotely located (i.e. at a central location in the hospital) in which case it is retrieved via an 40 Ethernet connection. When the SPOC application 523, 524, 526 is retrieved and loaded into RAM 414, the newly connected module 210, 212, 214, 250, 260 is coupled to it. The newly connected patient monitoring and/or treatment module 210, 212, 214, 250, 260 then is controlled by the central unit 45 300 and begins functioning.

As described above, a patient monitoring and/or treatment module 210, 212, 214, 250, 260 is sometimes removed from a central unit 300 in one location and reconnected to a central unit 300 at a different location (FIG. 3, FIG. 4). When, a 50 patient monitoring and/or treatment module 210, 212, 214, 250, 260 is reconnected to a central unit 300, the operating system 506 advantageously detects its presence and identifies the SPOC 523, 524, 526 required to control it. If the required SPOC 523, 524, 526 is already loaded, then it is coupled to the 55 newly connected module 210, 212, 214, 250, 260. If the required SPOC 523, 524, 526 is not already loaded, it is retrieved from a mass storage device, as described above.

A system described above integrates passive patient monitoring modules 210 (FIG. 3) and active treatment modules 60 212, 214, 250, 260 (infusion pumps, ventilators, anesthesiology equipment, incubators etc.) with a central unit 300 and associated system software 500 which receives physiological parameter data and operational status information from and supplies control information to both types of modules. The 65 software 500 permits modules to be disconnected from, and reconnected to the central unit 300. The software 500 also

24

permits interoperation of two or more of the modules cooperatively. The system reduces human error, improves speed of automatic adaptation of treatment, and of adapting treatment where human intervention is involved. In addition, the system improves the speed and accuracy of generating alerts, which may be crucial in a critical care unit such as an operating room. The system also saves space and cost, combines and groups alarms, provides consolidated documentation, facilitates module transportation and facilitates user operation. It reduces the problems presented to a healthcare worker in having to control multiple independent pieces of equipment. Because the modules may bidirectionally communicate with each other, tasks of supplying monitoring parameters to therapeutic modules, previously done manually, are advantageously accomplished automatically reducing human error. The critical care system may employ rules and programmed instruction governing addition of modules to the system. The integrated critical care system advantageously also provides a consistent user interface in both look and feel for the patient monitoring and therapeutic and life sustaining modules. This facilitates user friendly operation and reduces training required to educate a healthcare worker to operate the system compared to individual modules.

TABLE 1

Functions Waveform support Parameters Signal Group Support Alarm Support
Parameters Signal Group Support
Event Support Reporting Support Trend Support Trend Support GUI Components Deployment Support Diagnostics Peripheral Support Help Screen Layout Support Safety and Availability Hospital Network and Interface and Support Critical Care Network Interface and Support Patient Area Network Support Security User/Setups Configuration Support Patient Data/State Support Lifetime Management Database Real-time Infrastructure Communication Mechanisms
IT and Third Party App Support Etc Real-time Waveforms Real-time Measurements Real-time Alarm Behavior, Display and Control Home-screen Alarm Limits Trends Events Alarm History Remote/Bed to Bed View Calculations Strip Recordings Real-time Loops Real-time Flow Meters Demographics Patient Transfer Network Transfer Remote Control Monitor/Patient State Handling SW Option Handling Patient Context User Context Vital View Module/Patient Configuration/Setups

26 TABLE 1-continued

pressure exceeding the selected first percentage threshold and a fall in said cardiac output exceeding the

	TABLE 1-continued	_		TABLE 1-continued
SW Component	Functions	_	SW Component	Functions
	Patient Category			Agas monitoring
	Full Disclosure Application Selection and Configuration Tools	5		Plug and play of a-gases Inspiratory control
	Flight Recorder			Expiratory control
	Wireless Control			MAK monitor
	Remote Keypad Handling			Quantitative anesthesia
	Battery Management			Localization
	Measurement Setup and Priority	10		Etc
	Message Management		Fluid SPOC	TCI
	Print Screen Taskcards			TIVA PCA
	Localization			Localization
	Etc			Etc
Ventilation	PO1	15	CDPOC's	Anesthesia
Management and Gas	IntrPEEP	13		No agas without gas flow
Monitoring SPOC	Sigh			Acone
	Suction			Open Lung Tool
	Nebulize			Electrical Impedance Tomography (EIT)
	IMV (as example for a breathing mode) Recruitment			Respiratory Systolic Variation Test (RSVT) NICO
	Lung functions	20		Lung Mechanics Calculation (LMC)
	Smart Care			Automatic Lung Parameter Estimator (ALPE)
	NIV			Advanced Cardiopulmonary Integration Screens
	Monitor Respiratory System			BiPAP
	Insp/Exsp Hold			SMART Alarms
	NIF			SmartCare
	RSB	25		Localization
	RC		0.1 4 11 7	Etc
	CO2 Monitoring (including VCO and VDS)		Other Applications	IT ChartAssist
	Leakage Compensation Nurse Call			Remote View
	ILV			MegaCare
	HF	30		BU-IT
	Airway Temperature	50		Localization
	Flow and airway pressure monitoring			Etc
	Oxygen			Imaging
	Localization			2D
	Etc			3D
Monitor SPOC	ST Measuring Points	35		Virtual Film Sheet
	OCRG EEG Power Spectra			Patient Browser Dicom Query/Retrieve
	Cardiac Output			Localization
	Wedge			Etc
	Monitor Reports			Third Party
	Respiratory Mechanics	40		MagicWeb
	Surgical Display	40		Cypress
	MIB Management			Localization
	ECG Control			Etc.
	Invasive Pressure Control			
	SPO2 Control Respiration Control			
	Body Temperature Control	45	What is claime	ed is:
	NIBP Control		1. A method	for managing patient ventilator operation
	EEG Control		comprising the a	
	Transcutaneous Blood Gas Control			ventilation maneuver using a patient treat
	End Tidal CO2 Control			
	Arrhythmia Control		ment modul	
	ECG Lead Management	50		patient monitoring module data from at leas
	Fractional Inspired O2 Control MultiGas Control		one paramet	ter sensor, said data representing at least one
	Export Protocol Management		of arterial b	blood pressure, cardiac output, and ST seg-
	OR Mode		ment level of	of a patient:
	Monitor Setup			percent fall between first sensed data repre
	Nurse Call	5.5		east one of the arterial blood pressure and
	Auto Dual View	55		
	Auto Source Switching			out and subsequent sensed data correspond
	Localization			least one of the arterial blood pressure and
~	Etc			out using a central processor communicating
Anesthesia Gas	Air, oxygen, and N2O control		and control	ling the patient monitoring module and the
Mixing SPOC	Carrier gas selection	60		ment module;
	ORC (Young)	0.0		percent fall to at least one of a selected firs
	(Xenon) Fresh gas flow			
	Low and minimal flow		percentage	threshold corresponding to arterial blood
	Monitors gas supply			d a selected second percentage threshold cor
	Consumption monitoring incl. Prices		responding	to cardiac output using the central processor
	Agas control	65	in response to	at least one of a fall in said arterial blood
	Warm-up			ceeding the selected first percentage thresh
	-			fall in said cardiac output exceeding the

27

selected second percentage threshold, analyzing ST segment level of the patient using the central processor;

- in response to said ST segment level indicating no heart damage, using the central processor to adaptively alter at least one of the selected first percentage threshold and 5 the selected second percentage threshold to a selected third percentage threshold that is greater than the selected first percentage threshold or a selected fourth percentage threshold that is greater than the selected second percentage threshold; and
- in response to said ST segment level indicating possible heart damage, using the central processor to adaptively alter said ventilation maneuver.
- 2. The method of claim 1, wherein said adaptively altering said ventilation maneuver comprises at least one of (a) terminating the ventilation maneuver, (b) altering respiratory volume, and (c) altering respiratory pressure.
- 3. The method of claim 1, wherein said data representing at least one of arterial blood pressure, cardiac output, and ST segment level of a patient is averaged.
 - 4. The method of claim 1, further comprising: generating an alarm in response to the received data representing at least one of arterial blood pressure, cardiac output, and ST segment level of a patient.
- 5. The method of claim 1, wherein the ventilator maneuver 25 is at least one of a recruitment maneuver and a low flow positive ventilation (PV) maneuver.
- **6**. The method of claim **5**, wherein the recruitment maneuver is selected from the group consisting of at least one of regular sighs, sustained inflations, successively increased 30 positive end expiratory pressure (PEEP), and successively increased inspiratory pressure.
- 7. The method of claim 1, wherein said step of adaptively altering said ventilation maneuver comprises limiting the ventilation maneuver at a rate based on a degree of estimated 35 heart damage as indicated by said ST segment level.
- **8.** A method for managing patient ventilator operation comprising:
 - performing a ventilation maneuver using a patient treatment module;
 - receiving by a patient monitoring module data from at least one sensor representing arterial blood pressure;
 - receiving by the patient monitoring module data from said at least one sensor representing cardiac output;
 - calculating a percent fall between first sensed data representing at least one of the arterial blood pressure and the cardiac output and subsequent sensed data corresponding to the at least one of the arterial blood pressure and the cardiac output using a central processor communicating and controlling the patient monitoring module 50 and the patient treatment module;
 - comparing the percent fall to at least one of a selected first percentage threshold corresponding to arterial blood pressure and a selected second percentage threshold corresponding to cardiac output using the central processor 55 communicating and controlling the patient monitoring module and the patient treatment module;
 - in response to the at least one of a fall in said arterial blood pressure exceeding the selected first percentage threshold and a fall in said cardiac output exceeding the 60 selected second percentage threshold, analyzing received ST segment level of a patient using the central processor:
 - in response to said ST segment level indicating no heart damage, using the central processor to adaptively alter at 65 least one of the selected first percentage threshold and the selected second percentage threshold to a selected

28

- third percentage threshold that is greater than the selected first percentage threshold or a selected fourth percentage threshold that is greater than the selected second percentage threshold; and
- in response to said ST segment level indicating possible heart damage, using the central processor to limit said ventilation maneuver at a rate based on a degree of estimated heart damage indicated by said ST segment level.
- **9**. The method of claim **8**, wherein at least one of the data representing the arterial blood pressure and the data representing the cardiac output is averaged.
 - 10. The method of claim 8, further comprising: generating an alarm in response to the received data representing at least one of arterial blood pressure and cardiac output.
- 11. The method of claim 8, wherein the ventilation maneuver is at least one of a recruitment maneuver and a low flow positive ventilation (PV) maneuver.
 - 12. The method of claim 11, wherein the recruitment maneuver is selected from the group consisting of at least one of regular sighs, sustained inflations, successively increased positive end expiratory pressure (PEEP), and successively increased inspiratory pressure.
 - 13. The method of claim 8, wherein said step of limiting the ventilation maneuver comprises switching to low flow expiration while continuing said ventilation maneuver.
 - 14. A system for managing patient ventilator operation, comprising:
 - a patient monitoring module for receiving data from at least one sensor, said data representing at least one of arterial blood pressure, cardiac output, and ST segment level of a patient;
 - a patient treatment module for providing signals for adaptively altering a ventilation maneuver performed on the patient by a patient ventilator;
 - a central processor communicating and controlling the patient monitoring module and the patient treatment module, the central processor configured for
 - calculating a percent fall between first sensed data representing at least one of the arterial blood pressure and cardiac output and subsequent sensed data corresponding to the at least one of the arterial blood pressure and cardiac output;
 - comparing the percent fall to at least one of a selected first percentage threshold corresponding to arterial blood pressure and a selected second percentage threshold corresponding to cardiac output;
 - in response to at least one of a fall in said arterial blood pressure exceeding the selected first percentage threshold and a fall in said cardiac output exceeding the selected second percentage threshold, analyzing ST segment level data of the patient;
 - in response to ST segment level indicating no heart damage, adaptively altering at least one of the selected first percentage threshold and the selected second percentage threshold to a selected third percentage threshold that is greater than the selected first percentage threshold or a selected fourth percentage threshold that is greater than the selected second percentage threshold; and
 - in response to ST segment level indicating possible heart damage, adaptively altering said ventilation maneuver
 - 15. The system of claim 14, wherein adaptively altering said ventilation maneuver comprises at least one of (a) termi-

nating the ventilation maneuver, (b) altering respiratory volume, and (c) altering respiratory pressure.

- 16. The system of claim 14, wherein said data representing at least one of arterial blood pressure, cardiac output, and ST segment level of the patient is averaged.
 - 17. The system of claim 14,
 - wherein the central processor is further configured for generating an alarm in response to the received data representing at least one of arterial blood pressure, cardiac output and ST segment level of the patient.
- 18. The system of claim 14, wherein the ventilation maneuver is at least one of a recruitment maneuver and a low flow positive ventilation (PV) maneuver.
- 19. The system of claim 18, wherein the recruitment maneuver is selected from the group consisting of at least one 15 of regular sighs, sustained inflations, successively increased positive end expiratory pressure (PEEP), and successively increased inspiratory pressure.
- **20**. The system of claim **14**, wherein adaptively altering said ventilation maneuver comprises limiting the ventilation 20 maneuver at a rate based on a degree of estimated heart damage as indicated by said ST segment level.

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